

A nonstandard higher-order variational model to speckle noise removal and thin-structure detection

Hamdi Houichet* Anis Theljani[†] Maher Moakher* Badreddine Rjaibi*

June 19, 2017

Abstract

In this work, we propose a multiscale approach for a nonstandard higher-order PDE based on the $p(\cdot)$ -Kirchhoff energy. First, we consider a topological gradient approach for a semi-linear case in order to detect important object of image. Then, we consider a fully nonlinear $p(\cdot)$ -Kirchhoff equation with variables exponent functions that are chosen adaptively based on the map furnished by the topological gradient in order to preserve important features of the image. Then, we consider the split Bregman method for the numerical implementation of our proposed model. We compare our model with other classical variational approaches such that the TVL and biharmonic restoration models. Finally, we present some numerical results to illustrate the effectiveness of our approach.

Keywords: Inverse problems, regularization procedures, $p(\cdot)$ -Kirchhoff, topological gradient, split Bregman.

1 Introduction

Image restoration is a fundamental task in image processing and it arises in diverse fields (geophysics, optics, medical imaging, etc). In this work, we are interested in the restoration of images highly corrupted with multiplicative noise. It is a challenging task in various fields and particularly in ultrasound medical imaging. The reason is that ultrasound images are strongly influenced by the quality of data usually corrupted with Rayleigh-distributed multiplicative noise. The latter is so-called speckle noise [30, 31, 34] and usually affects image analysis methods by making important features hard to detect. We aim to reconstruct an image $u : \Omega \rightarrow \mathbb{R}$ from an observed one $f : \Omega \subset \mathbb{R}^2 \rightarrow \mathbb{R}$ which is degraded and contaminated by noise. The degradation model that we consider is the following:

$$f = u + g(u)\eta, \quad (1)$$

where $\eta : \Omega \rightarrow \mathbb{R}$ is a positive function that follows the Rayleigh-distribution. The function $g(\cdot)$ encodes the noise type in such a way that $g(u) \equiv 1$ in the case of additive Gaussian noise, i.e., $f = u + n$, and $g(u) = \sqrt{u}$ in the case of speckle (multiplicative) noise. The reconstruction problem based on model (1) is an ill-posed inverse problem and thus regularization techniques are needed to overcome ill-posedness. Generally, the regularization technique turns the reconstruction problem based on model (1) into a well-posed optimization one where the energy to be minimized is the sum of a regularization

*University of Tunis El Manar, National Engineering School at Tunis, Laboratory for Mathematical and Numerical Modeling in Engineering Science, B.P. 37, 1002 Tunis-Belvédère, Tunisia. Emails: hamdi.houichet@enit.utm.tn (H. Houichet), maher.moakher@enit.utm.tn (M. Moakher) and badreddine.rjaibi@lamsin.rnu.tn (B. Rjaibi).

[†]Liverpool Centre for Mathematics in Healthcare, Department of Mathematical Sciences, University of Liverpool, Liverpool, UK. Email: a.theljani@liverpool.ca.uk.

term (mostly a semi-norm of a functional space fixed a priori) and a data fitting term. In general, the well-posed minimization problem has the following form:

$$\min_{\{u>0; u \in \mathcal{H}\}} \left\{ \mathcal{J}(u) := J(u) + \lambda \int_{\Omega} \left(\frac{f-u}{g(u)} \right)^2 dx \right\}, \quad (2)$$

The first part in energy $\mathcal{J}(\cdot)$ is a regularization term, the second one is the fitting term, λ is a positive weight which controls the trade-off between them and \mathcal{H} is a space of the solution.

The main issue is how to choose the “best” regularization term which can selectively smooth a noisy image without losing significant features such as edges and thin structures. In various recent works [9, 10, 37], higher-order derivatives have been used to damp oscillations and to avoid stair-casing effect of second order derivatives. In [13], Chan, Marquina and Mulet used the following regularizer:

$$J_{CMM}(u) = \int_{\Omega} \left(|\nabla u| + \frac{(\Delta u)^2}{|\nabla u|^3} \right) dx,$$

where ∇ and Δ denote the gradient and the Laplace operators, respectively. Another prominent regularizer using higher-order derivatives was proposed by You-Kaveh [44] by considering:

$$J_{YK}(u) = \int_{\Omega} f(|\Delta u|) dx,$$

which, when $f(s) = s$, leads to a nonlinear (TV-like) higher-order PDE and when $f(s) = s^2$ to the biharmonic equation -plenty regularization. In this work, we consider a new regularization term defined by a regularizer which is a compromise between the extreme cases $f(s) = s$ and $f(s) = s^2$. More precisely, we consider the following regularizer:

$$J^{p,q}(u) = \alpha \int_{\Omega} \frac{1}{p(x)} |\Delta u|^{p(x)} dx + \beta \int_{\Omega} \frac{1}{q(x)} |\nabla u|^{q(x)} dx, \quad (3)$$

where the functions $p(\cdot)$ and $q(\cdot)$ are defined on Ω and satisfy $1 < p(\cdot), q(\cdot) \leq 2$. Nonstandard PDEs with variable exponent $p(\cdot)$, specially for the p -Laplace equation, were considered in several works (see [8, 22, 33]). A lot of research recently studied partial differential equations and variational problems with $p(\cdot)$ -growth conditions which arise in electro-rheological fluids [38], elasticity theory [45] and image processing [14, 28, 32].

The smoothness propriety in these nonstandard PDEs is driven by the variables exponent $p(\cdot)$ and $q(\cdot)$. The approach that we propose automatically balances between L^1 -Laplacian (respectively L^1 -gradient) and L^2 -Laplacian (respectively L^2 -gradient) regularization effects. Thus, by giving the variable exponent $p(\cdot)$ and $q(\cdot)$ the possibility to take values between 1 and 2 we allow to slow diffusion near edges, and enhance diffusion in smooth regions. This choice avoids over smoothing and stair-casing artifact effects of L^2 - and L^1 -regularization. However, a common question is how to choose the values of the exponents $p(\cdot)$ and $q(\cdot)$? A classical idea is to make an adaptive choice for $p(\cdot)$ and $q(\cdot)$. We identify the important features using classical edge and thin-structure detector and then we vary the exponents $p(\cdot)$ and $q(\cdot)$, according to edge-map, in the restoration process by considering a fully nonlinear $p(\cdot)$ -Kirchhoff model for $1 < p(\cdot), q(\cdot) \leq 2$. For edge and thin-structure detection task, we consider the topological gradient approach (see for Laplace, [3, 7]) and thin-structures (see [6, 16] for biharmonic equation). The natural choice is to consider the nonlinear $p(\cdot)$ -Kirchhoff energy. Unfortunately, it has not yet been studied thoroughly for $p(\cdot)$ -biharmonic operators we don't address it in this work. However, it was recently studied in [6, 16] for biharmonic operator with very satisfactory result in the detection of fine features (arteries, filaments, internal organ, etc.). We extend the result obtained in [7, 6, 16] by considering as topological gradient for the particular case $p(\cdot) \equiv q(\cdot) \equiv 2$.

This paper is organized as follows. In Section 2, we fix notations and recall useful results for the generalized Lebesgue/Sobolev spaces. In Section 3, we prove, by standard variational techniques, the existence and uniqueness of the minimizer of the energy functional (2). In Section 4, we give the formula of the topological gradient for $p(\cdot) \equiv q(\cdot) \equiv 2$. In section 5, we present the adaptive algorithm and we present the split Bregman scheme for the restoration process. Finally, in Section 6, we treat some numerical examples to test its efficiency and robustness.

2 Preliminaries and notations

Before going further, we recall some useful definitions and results about the variable-exponent generalized Lebesgue and Sobolev spaces $L^{p(\cdot)}(\Omega)$ and $W^{k,p(\cdot)}(\Omega)$. For more details, we refer the reader to [15, 17, 18, 20, 21]. For a bounded Lipschitz open set $\Omega \subset \mathbb{R}^N$ with sufficiently smooth boundary $\partial\Omega$, we define the variable-exponent generalized Lebesgue space $L^{p(\cdot)}(\Omega)$ as follows:

$$L^{p(\cdot)}(\Omega) := \left\{ u : \Omega \rightarrow \mathbb{R} \text{ measurable and } \int_{\Omega} |u(x)|^{p(x)} dx < \infty \right\},$$

where $p(\cdot) \in C(\overline{\Omega})$ be a measurable function, called variable exponent on Ω and satisfy the following condition:

$$1 < p^- := \inf_{x \in \Omega} p(x) \leq p(x) \leq p^+ := \sup_{x \in \overline{\Omega}} p(x) \leq 2. \quad (4)$$

$L^{p(\cdot)}(\Omega)$ is a normed linear space equipped with the Luxemburg norm:

$$\|u\|_{L^{p(\cdot)}} = \inf \left\{ \varrho > 0 : \int_{\Omega} \left| \frac{u(x)}{\varrho} \right|^{p(x)} dx \leq 1 \right\}.$$

The Sobolev space with variable exponent $W^{k,p(\cdot)}(\Omega)$ is defined as:

$$W^{k,p(\cdot)}(\Omega) = \left\{ u \in L^{p(\cdot)}(\Omega) : D^{\xi}u \in L^{p(\cdot)}(\Omega), |\xi| \leq k \right\},$$

where $D^{\xi}u = \frac{\partial^{|\xi|}}{\partial x_1^{\xi_1} \partial x_2^{\xi_2} \dots \partial x_N^{\xi_N}} u$ with $\xi = (\xi_1, \dots, \xi_N)$ is a multi-index and $|\xi| = \sum_{i=1}^N \xi_i$. The space $W^{k,p(\cdot)}(\Omega)$, is equipped with the norm:

$$\|u\|_{k,p(\cdot)} := \sum_{|\xi| \leq k} \|D^{\xi}u\|_{L^{p(\cdot)}}.$$

Both $(L^{p(\cdot)}(\Omega), \|\cdot\|_{L^{p(\cdot)}})$ and $(W^{k,p(\cdot)}(\Omega), \|\cdot\|_{k,p(\cdot)})$ are separable, reflexive and uniformly convex Banach spaces [21].

Lemma 2.1 [15] (**Generalized Poincaré's inequality**). *If Ω is a Lipschitz domain, then, there exists a constant $C > 0$ such that for all $u \in W^{1,p(\cdot)}(\Omega)$:*

$$\left\| u - \frac{1}{|\Omega|} \int_{\Omega} u dx \right\|_{L^{p(\cdot)}} \leq C \|\nabla u\|_{L^{p(\cdot)}}.$$

Remark 2.1 *We consider the following space $X = \{u \in W^{2,p(\cdot)}(\Omega) \mid \frac{\partial u}{\partial n} = 0\}$. The norm $\|u\|_{2,p(\cdot)}$ is equivalent to the norm $\|u\|_X = \|\Delta u\|_{L^{p(\cdot)}}$ in the spaces $W^{2,p(\cdot)}(\Omega)$ and X . Moreover, $(W^{2,p(\cdot)}(\Omega); \|\cdot\|_X)$ and $(X; \|\cdot\|_X)$ are Banach, separable and reflexive spaces.*

We consider the space $\tilde{W}^{1,p(\cdot)}(\Omega) = \{u \in W^{1,p(\cdot)}(\Omega); \int_{\Omega} (u - f) dx = 0\}$, and the potentials $J^p(\cdot) = \int_{\Omega} \frac{1}{p(x)} |\Delta \cdot|^{p(x)} dx$ and $J^q(\cdot) = \int_{\Omega} \frac{1}{q(x)} |\nabla \cdot|^{q(x)} dx$. Then, we have the following proposition:

Proposition 2.2 For sequences $(u_n)_n \in W^{2,p(\cdot)}(\Omega)$ and $(v_n)_n \in \tilde{W}^{1,q(\cdot)}(\Omega)$, as $n \rightarrow \infty$ we have:

$$(a) \|u_n\|_{2,p(\cdot)} \rightarrow \infty \Leftrightarrow J^p(u_n) \rightarrow \infty.$$

$$(b) \|v_n\|_{W^{1,q(\cdot)}} \rightarrow \infty \Leftrightarrow J^q(v_n) \rightarrow \infty.$$

Proof: The proof of this proposition is similar to the proof of Theorem 1.3 in [21]. □

3 Mathematical formulation of the problem

Let $p(\cdot), q(\cdot) \in C(\bar{\Omega})$ such that these two functions are not related to each other. For our purpose, they just have to satisfy (4). Adapted to our specific problem here, we introduce the working space $\mathcal{H}^{p(\cdot)}$ by:

$$\mathcal{H}^{p(\cdot)}(\Omega) = X \cap W^{1,q(\cdot)}(\Omega),$$

which can be equipped with the norm $\|\cdot\| = \|\Delta \cdot\|_{L^{p(\cdot)}} + \|\nabla \cdot\|_{L^{q(\cdot)}}$.

In this paper, we discuss the image restoration problem, using model (2), based on the minimization of the following energy:

$$\mathcal{J}(u) = \left\{ J^{p,q}(u) + \lambda \int_{\Omega} W(u, f) \, dx \right\}, \quad (5)$$

where W is the locally Lipschitz continuous function defined by:

$$W(s, z) := \left(\frac{z - s}{g(s)} \right)^2 \quad \forall s, z > 0.$$

For any $s > 0$, $W(s, \cdot)$ is a strict convex function. Moreover, the first-derivative of W with respect to s is

$$\frac{\partial W}{\partial s}(s, z) = \phi(s)(s - z) \quad \text{where} \quad \phi(s) = \frac{g(s) + (s - z)g'(s)}{g(s)^3}$$

is positive when $0 < \inf z \leq s \leq \sup z$.

Moreover, let $m, M > 0$ such that $m \leq s \leq M$, the following inequality hold

$$\frac{\partial W}{\partial s}(m, z) \leq 0 \quad \text{and} \quad \frac{\partial W}{\partial s}(M, z) \geq 0. \quad (6)$$

For brevity, we sometimes write $W(\cdot)$ for $W(\cdot, f)$ and $D_u W(\cdot, f)$ for $W'(\cdot, f)$.

3.1 Existence and uniqueness of solution

In the sequel, we establish the well-posedness of the following minimization problem:

$$\min_{u \in \mathcal{H}^{p(\cdot)}(\Omega)} \{ \mathcal{J}(u) \mid \int_{\Omega} (f - u) \, dx = 0 \}. \quad (7)$$

Proposition 3.1 The minimization problem (7) admits a unique minimizer u in $\mathcal{H}^{p(\cdot)}(\Omega)$. Moreover, we have

$$0 < \inf_{\Omega} f \leq u \leq \sup_{\Omega} f. \quad (8)$$

Proof: First, it easy to see that the energy $\mathcal{J}(\cdot)$ is strictly convex and weakly lower semi-continuous in the space $\mathcal{H}^{p(\cdot)}(\Omega)$. Let us consider a minimizing sequence $(u_n)_n \subset H(\Omega) := \{u > 0, u \in \mathcal{H}^{p(\cdot)}(\Omega)\}$ of $\mathcal{J}(\cdot)$, i.e.,

$$\mathcal{J}(u_n) \xrightarrow{n \rightarrow \infty} \inf_{u \in \mathcal{H}^{p(\cdot)}(\Omega)} \mathcal{J}(u).$$

We denote by $m := \inf_{\Omega} f$ and $M := \sup_{\Omega} f$ and let $(v_n)_n \subset H(\Omega)$ be the sequence defined by $v_n = \min(u_n, M)$ and set $D = \{x \in \Omega; u_n(x) \geq M\}$. Since on $\Omega \setminus D$ we have $u_n = v_n$, it follows that

$$\begin{aligned} \mathcal{J}(v_n) - \mathcal{J}(u_n) = & -\alpha \left(\int_D \frac{1}{p(x)} \left(|\Delta v_n|^{p(x)} + |\Delta u_n|^{p(x)} \right) dx \right) + \int_D (W(M) - W(u_n)) dx \\ & - \beta \left(\int_D \frac{1}{p(x)} \left(|\nabla v_n|^{q(x)} - |\nabla u_n|^{q(x)} \right) dx \right). \end{aligned} \quad (9)$$

Using the convex property of W and the second inequality in (6), we can write:

$$\int_D (W(M) - W(u_n)) dx \leq - \int_D D_u W(M)(M - u_n) \leq 0.$$

It follows that $\mathcal{J}(v_n) \leq \mathcal{J}(u_n)$ and $(v_n)_n$ is also a minimizing sequence satisfying $v_n \leq M$. The same analysis goes for $w_n = \max(u_n, m)$ and we also obtain that $(u_n)_n$ satisfying $m \leq u_n$. Therefore, we can assume, without restriction, that $m \leq u_n \leq M$. In addition, since $\int_{\Omega} (u - f) dx = 0$, from the previous inequality, Proposition 2.2 and the Poincaré's inequality, we easily get the sequence $(u_n)_n$ is uniformly bounded in $\mathcal{H}^{p(\cdot)}(\Omega)$. Thus, there exists a subsequence, still denoted $(u_n)_{n \in \mathbb{N}}$, such that $u_n \xrightarrow{n \rightarrow \infty} u$ weakly in $\mathcal{H}^{p(\cdot)}(\Omega)$ and the limit u is a minimizer of $\mathcal{J}(\cdot)$ and it fulfills inequality (8). The uniqueness comes from the strict convexity of $\mathcal{J}(\cdot)$. □

In terms of diffusion PDEs, the solution u of the minimization problem (7) is a weak solution of the Euler-Lagrange equation:

$$\begin{cases} \alpha \Delta (|\Delta u|^{p(x)-2} \Delta u) - \beta \operatorname{div}(|\nabla u|^{q(x)-2} \nabla u) + 2\lambda D_u W(u, f) = 0, & \text{in } \Omega, \\ \frac{\partial \Delta u}{\partial n} = \frac{\partial u}{\partial n} = 0, & \text{on } \partial \Omega. \end{cases} \quad (10)$$

The assumption that $\int_{\Omega} (u - f) dx = 0$ is automatically satisfied. In fact, integrating the PDE in (10) in space and using integration by parts and the boundary conditions, we get that $\int_{\Omega} \phi(u)(u - f) dx = 0$, thus the result is easily obtained by using the positivity of u and f .

The operator $\Delta (|\Delta u|^{p(x)-2} \Delta u) := \Delta_{p(\cdot)}^2 u$ is of fourth-order and usually called the $p(\cdot)$ -biharmonic operator [1, 19]. In the particular case where $p(\cdot) \equiv q(\cdot) \equiv 2$, we get a linear fourth-order PDEs corresponding to the biLaplace operator. As mentioned in the introduction, we will consider the topological gradient in the particular case $p(\cdot) \equiv q(\cdot) \equiv 2$.

4 Important features detection via topological gradient method

Thin structure, like filament in 3-D or a point in 2-D, is an object that can be linked to a curve. For the edge detection the usual spatial gradient is classically used, but for the structures, it is not efficient [40, 41]. Thin structures have a profile in the form of the delta function, however, edges have a profile in the form of the Heaviside function. The edges have a jump of intensity through the discontinuity but the structure does not have a jump of intensity through the discontinuity more precisely the size of thin structures. The difficulties comes from the presence of noise and the fact that filaments are thin

or/and non regular. However, the topological gradient approach provides an accurate identification of these kind of discontinuities [6, 16].

In the sequel, we recall the basic idea of the topological gradient method. For a small parameter $\varepsilon > 0$, let Ω_ε be the perturbed domain of Ω obtained by creating a small hole $\omega_\varepsilon = \varepsilon\omega$ around the point $x \in \Omega$, i.e., $\Omega_\varepsilon = \Omega \setminus \omega_\varepsilon$, where ω is the fixed smooth open bounded subset in \mathbb{R}^2 . Let $J_\varepsilon(u_\varepsilon)$ is a cost functional where u_ε is a solution of a given PDE on the perturbed domain Ω_ε . Note that $J_0(u_0)$ where u_0 is the solution of the given PDE on the initial domain Ω . The variation of the cost functional, has the following asymptotic expansion:

$$J_\varepsilon(u_\varepsilon) - J_0(u_0) = \rho(\varepsilon)G(x_0) + o(\rho(\varepsilon)),$$

In this expansion, ρ is an explicit function such that $\rho(\varepsilon) \geq 0$ and $\lim_{\varepsilon \rightarrow 0} \rho(\varepsilon) = 0$, $G(x_0)$ is the topological gradient which does not depend on ε . To minimize the criterion $J_\varepsilon(\cdot)$, one has to create holes at some points where the topological gradient G is negative, which are regions of the important features to be detected.

In our approach, we define the following Fréchet differentiable cost functional which will be minimized outside the important features:

$$J(u) = \frac{\alpha}{2} \int_{\Omega} |\Delta u|^2 dx + \frac{\beta}{2} \int_{\Omega} |\nabla u|^2 dx, \quad (11)$$

The choice of this cost functional has two folds. First, second-order derivatives are mostly used in order to detect and preserve thin structures [6, 16, 5], points or filaments, where there is no jump across the intensity. Second, the classical gradient (first-order derivatives) usually gives a promising result in edge detection [3, 7, 2, 29]. The parameters α and β are positive constants that can be chosen so that either edges or thin-structures are privileged.

We assume that important features are modeled by cracks and that the perturbed domain $(\Omega_\varepsilon)_{\varepsilon \geq 0}$ is obtained by inserting a small family of insulating cracks $(\sigma_\varepsilon)_{\varepsilon \geq 0}$, where $\sigma_\varepsilon = \varepsilon\sigma(n)$ and σ is the fixed crack in Ω and n its unit outward normal.

The solution u_ε of the previous minimization problem fulfills the following optimality conditions:

$$\begin{cases} \alpha \Delta^2 u_\varepsilon - \beta \Delta u_\varepsilon + 2\lambda D_u W(u_\varepsilon, f) = 0, & \text{in } \Omega_\varepsilon, \\ \frac{\partial \Delta u_\varepsilon}{\partial n} = \frac{\partial u_\varepsilon}{\partial n} = 0, & \text{on } \partial\Omega_\varepsilon, \end{cases} \quad (12)$$

where $\Delta^2 := \Delta \cdot \Delta$ is the biLaplace operator and $\partial\Omega_\varepsilon = \partial\Omega \cap \bar{\sigma}_\varepsilon$.

The computation of the topological gradient for the cost function (11) is straightforward application of the analysis given in [6, 5, 4] and we have the following proposition.

Proposition 4.1 *Let u_0 be the solution of (12) with $\varepsilon = 0$. Then, we have the following topological gradient:*

$$G(x_0, n) = -\alpha \frac{2\pi}{3} \nabla^2 u_0(x_0)(n, n) \nabla^2 v_0(x_0)(n, n) - \beta \pi \nabla u_0(x_0) \cdot n \nabla v_0(x_0) \cdot n, \quad (13)$$

where v_0 solves the following adjoint equation:

$$\begin{cases} \alpha \Delta^2 v_0 - \beta \Delta v_0 + \lambda D_u^2 W(u_0, f) v_0 = -\alpha \Delta^2 u_0 + \beta \Delta u_0, & \text{in } \Omega_\varepsilon, \\ \frac{\partial \Delta v_0}{\partial n} = \frac{\partial v_0}{\partial n} = 0, & \text{on } \partial\Omega_\varepsilon, \end{cases} \quad (14)$$

and $D_u^2 W(s, z)$ is the second derivative of $s \mapsto W(s, z)$ evaluated at $s \in \mathbb{R}_+^*$.

Remark 4.1 *The adjoint equation (14) comes from the first optimality conditions for the Lagrangian :*

$$\mathcal{L}(u_0, v_0) = J(u_0) + \alpha \int_{\Omega} \Delta u_0 \Delta v_0 \, dx + \beta \int_{\Omega} \nabla u_0 \nabla v_0 \, dx + \lambda \int_{\Omega} D_u W(u_0, f) v_0 \, dx.$$

Equation (14) can be directly obtained by taking $\frac{\partial \mathcal{L}}{\partial u}(u_0, v_0) = 0$ and applying Green's formula. For background materials we refer the reader to, e.g. [11, 12, 23, 35, 39]. Moreover, the adjoint equation is linear and by applying the Lax-Milgram theorem, it has a unique solution $v \in H^2(\Omega)$.

Proposition 4.1 combines the results obtained previously for the case of the second- and fourth-order PDE. In addition, we can write:

$$G(x_0, n) = G^F(x_0, n) + G^S(x_0, n),$$

where

$$\begin{cases} G^S(x_0, n) = -\beta \pi \nabla u_0(x_0) \cdot n \nabla v_0(x_0) \cdot n, \\ G^F(x_0, n) = -\alpha \frac{2\pi}{3} \nabla^2 u_0(x_0)(n, n) \nabla^2 v_0(x_0)(n, n). \end{cases}$$

The quantity $G^S(x_0, n)$ corresponds to the topological gradient result of first-order derivatives (i.e., $\alpha = 0$) and it is sensitive to edges (see [7, 29]). It can be written as:

$$G^S(x_0, n_c) = \langle M(x) n, n \rangle_E,$$

where $\langle \cdot, \cdot \rangle_E$ is the Euclidean scalar product and $M(x)$ is the 2×2 symmetric matrix defined by:

$$M(x) = -\pi \frac{\nabla u_0(x) \nabla v_0(x)^T + \nabla v_0(x) \nabla u_0(x)^T}{2},$$

where $n = (\cos \theta, \sin \theta)$ is a unit normal to the crack and $\theta \in [0, \pi]$. On each point x_0 , $G^S(x_0, n)$ takes its minimal value when n is the eigenvector associated to the smallest eigenvalue e_{\min} of M . This value will be considered as the topological gradient indicator associated to the optimal orientation of the crack which is an edge of the image.

However, the quantity $G^F(x_0, n)$ is the topological gradient for fourth-order derivatives (i.e., $\beta = 0$) and it is sensitive to fine structures and points. It was proved in [16] that the quantity $G^F(x_0, n)$ can be written as:

$$G^F(x_0, \theta) = -\frac{2\pi}{3} P(\partial_{xx} u_0(x_0), \partial_{yy} u_0(x_0), \partial_{xy} u_0(x_0), \theta) P(\partial_{xx} v_0(x_0), \partial_{yy} v_0(x_0), \partial_{xy} v_0(x_0), \theta),$$

where $P : \mathbb{R}^4 \rightarrow \mathbb{R}$ is defined by:

$$P(x, y, z, \theta) = \frac{1}{2}(x + y) + \frac{1}{2}(x - y) \cos(2\theta) + z \sin(2\theta).$$

which is clearly π -periodical function with respect to θ .

5 Implementation

The smoothness of the solution is driven by the variable exponents $p(\cdot)$ and $q(\cdot)$ which will be chosen adaptively in order to slow diffusion near edges in order to sharpen and highlight them, and enhance diffusion in homogeneous regions. The restoration task is carried out in two steps: In an initial step, we use the topological gradient method for the biharmonic cost function (i.e. for $p(\cdot) \equiv q(\cdot) \equiv 2$),

to detect important features. In a second step, we use the information furnished by the topological gradient (calculated for $p(\cdot) \equiv q(\cdot) \equiv 2$) in order to vary the exponent $p(\cdot)$ in the restoration process by considering a $p(\cdot)$ -biharmonic model for $1 < p(\cdot), q(\cdot) \leq 2$. The particularity of topological gradient of being an efficient edge- and thin structure-detector makes it well suited to control and locally select the exponent using the following algorithm:

Algorithm 1 MAIN ALGORITHM

Given f and λ .

1. For $p(\cdot) \equiv 2$ and $q(\cdot) \equiv 2$, compute u and v which solve equations (12) and (14), respectively.
 2. Compute the topological gradient $G(x_0, n)$ for each point $x_0 \in \Omega$.
 3. Update $p(\cdot)$ and $q(\cdot)$ to obtain new exponents $p_a(\cdot)$ and $q_a(\cdot)$. Then, solve (10) for $p(\cdot) \equiv p_a(\cdot)$ and $q(\cdot) \equiv q_a(\cdot)$.
-

In order to update the exponents $p(\cdot)$ and $q(\cdot)$, we use the following formulas:

$$p_a(x) = 1 + \exp(-\kappa_1 |G^F(x, n)|), \quad q_a(x) = 1 + \exp(-\kappa_2 |G^S(x, n)|), \quad \forall x \in \Omega,$$

where $\kappa_1, \kappa_2 > 0$ are constants. In homogeneous regions, we have $G^F(x, n) \approx 0$, (respectively $G^S(x, n) \approx 0$) leading to a new exponent $p_a(x)$ (respectively $q_a(x)$) close to 2. Then, the model behaves like the biharmonic equation leading to strong diffusion and hence noise is damped. Near edges, $G^F(x, n)$ (respectively $G^S(x, n)$) is very important and therefore $p_a(x)$ (respectively $q_a(x)$) will be close to 1 which slows down diffusion. However, for such a choice of $p_a(\cdot)$ and $q_a(\cdot)$, equation (10) is strongly nonlinear. For that, we will use a split Bregman algorithm.

5.1 Split Bregman Algorithm

In [27], the authors proposed a new technique based on the Bregman iteration for solving non-smooth problems, particularly, L^1 -regularized problems. Originally, it was invented to solve ROF-model from Rudin, Osher and Fatemi model in image restoration. See also the works by Getreuer [24, 25, 26] which use the split Bregman method for TV denoising, deblurring and inpainting. After that, it was applied for more general problems such as higher-order models. In our case, the original energy functional (3) is a non-differentiable functional of u .

5.1.1 Discretization

We assume that our discrete images have $l \times c$ pixels, where l and c are the numbers of rows and columns in the image, respectively. We define the discrete operators and norms that will be used in the numerical implementation. We first consider the following discrete norms:

$$\left\{ \begin{array}{l} \|u\|_2 = \left(\sum_{i=1}^l \sum_{j=1}^c u(i, j)^2 \right)^{1/2}, \quad u : \{1, \dots, l\} \times \{1, \dots, c\} \longrightarrow \mathbb{R}, \\ \|m\|_p = \sum_{i=1}^l \sum_{j=1}^c \frac{1}{p(i, j)} |m(i, j)|^{p(i, j)}, \quad m : \{1, \dots, l\} \times \{1, \dots, c\} \longrightarrow \mathbb{R}, \\ \|n\|_q = \sum_{i=1}^l \sum_{j=1}^c \frac{1}{q(i, j)} (n_1(i, j)^2 + n_2(i, j)^2)^{q(i, j)/2}, \quad n : \{1, \dots, l\} \times \{1, \dots, c\} \longrightarrow \mathbb{R}^2. \end{array} \right. \quad (15)$$

For the discrete differential operators, we assume periodic boundary conditions for u . By choosing periodic boundary conditions, the action of each of the discrete differential operators can be regarded as a circular convolution of u and allows the use of fast Fourier transform (see [36, 42, 43] for more details). We consider the discrete first- and second-order derivatives D_x , D_y , D_{xx} and D_{yy} as operators from $\mathbb{R}^{l \times c}$ to \mathbb{R} . The discrete gradient is $\nabla u = (D_x u, D_y u)$ where D_x and D_y are forward difference operators defined as follows:

$$D_x = \begin{cases} u(i, j+1) - u(i, j) & 1 \leq i \leq l, 1 \leq j < c, \\ u(i, 1) - u(i, j) & 1 \leq i \leq l, j = c, \end{cases}$$

$$D_y = \begin{cases} u(i+1, j) - u(i, j) & 1 \leq i < l, 1 \leq j \leq c, \\ u(1, j) - u(i, j) & i = l, 1 \leq j \leq c. \end{cases}$$

We also define the following backward difference operators

$$\overleftarrow{D}_x = \begin{cases} u(i, j) - u(i, c) & 1 \leq i \leq l, j = 1, \\ u(i, j) - u(i, j-1) & 1 \leq i \leq l, 1 < j \leq c, \end{cases}$$

$$\overleftarrow{D}_y = \begin{cases} u(i, j) - u(l, j) & i = 1, 1 \leq j \leq c, \\ u(i, j) - u(i-1, j) & 1 < i \leq l, 1 \leq j \leq c. \end{cases}$$

Then, the discrete divergence operator is given by $\text{div } n = \overleftarrow{D}_x n_1 + \overleftarrow{D}_y n_2$. We also define the following second-order discrete differential operators:

$$D_{xx} = \begin{cases} u(i, c) - 2u(i, j) + u(i, j+1) & 1 \leq i \leq l, j = 1, \\ u(i, j-1) - 2u(i, j) + u(i, j+1) & 1 \leq i \leq l, 1 < j < c, \\ u(i, j-1) - 2u(i, j) + u(i, 1) & 1 \leq i \leq l, j = c, \end{cases}$$

$$D_{yy} = \begin{cases} u(l, j) - 2u(i, j) + u(i+1, j) & i = 1, 1 \leq j \leq c, \\ u(i-1, j) - 2u(i, j) + u(i+1, j) & 1 < i < l, 1 \leq j \leq c, \\ u(i-1, j) - 2u(i, j) + u(1, i) & i = l, 1 \leq j \leq c, \end{cases}$$

$$D_{xy} = \begin{cases} u(i, j) - u(i+1, j) - u(i, j+1) + u(i+1, j+1) & 1 \leq i < l, 1 \leq j < c, \\ u(i, j) - u(1, j) - u(i, j+1) + u(1, j+1) & i = l, 1 \leq j < c, \\ u(i, j) - u(i+1, j) - u(i, 1) + u(i+1, 1) & 1 \leq i < l, j = c, \\ u(i, j) - u(1, j) - u(i, 1) + u(1, 1) & i = l, j = c. \end{cases}$$

Then, the discrete Laplace operator is given by $\Delta u = D_{xx} + D_{yy}$.

5.1.2 Split Bregman iterations

The split Bregman method applied to (3) consists in introducing auxiliary variables v , m and n and then solving the following constrained minimization problem:

$$\min_{u, v, m, n} \mathcal{J}_d(u, v, m, n), \text{ such that } v = u, \quad \Delta v = m, \quad \nabla v = n, \quad (16)$$

where

$$\mathcal{J}_d(u, v, m, n) = \|m\|_p + \|n\|_q + \lambda \sum_{i=1}^l \sum_{j=1}^c \frac{(u(i, j) - f(i, j))^2}{u(i, j)}.$$

Remark 5.1 *It appears on first sight that it is not necessary to introduce the auxiliary variables v . However, this auxiliary variable is crucial since it allows to avoid solving a nonlinear problem which will be faced in the u -subproblem due to the nonlinear data fitting term $W(u, f)$.*

Split Bregman iterations consist in solving the constrained minimization problem (16) using the iterative scheme summarized in the following steps:

Algorithm 2 SPLIT BREGMAN ITERATIONS

Initialization: $u_1 = u_0$, $v_1 = u_0$, $\Delta u_0 = m_1$, $\nabla u_0 = n_1$, $b_0^0 = 1$, $b_0^1 = 1$ and $b_0^2 = 1$.

$$\begin{aligned} [u_{k+1}, v_{k+1}, m_{k+1}, n_{k+1}] &= \operatorname{argmin}_{u,v,m,n} \mathcal{J}_d(u, v, m, n) + \frac{\lambda_0}{2} \|b_k^0 + u - v\|_2^2 \\ &\quad + \frac{\lambda_1}{2} \|b_k^1 + \Delta v - m\|_2^2 + \frac{\lambda_2}{2} \|b_k^2 + \nabla v - n\|_2^2, \\ b_{k+1}^0 &= b_k^0 + u_{k+1} - v_{k+1}, \\ b_{k+1}^1 &= b_k^1 + \Delta v_{k+1} - m_{k+1}, \\ b_{k+1}^2 &= b_k^2 + \nabla v_{k+1} - n_{k+1}. \end{aligned}$$

It is difficult to minimize the energy (16) with respect to all variables jointly, thus in every iteration we split it into four separate subproblems, each of which can be solved quickly. We apply an alternating minimization iterative procedure, namely, for $k = 0, 1, \dots$, we solve successively:

$$\left\{ \begin{array}{l} \text{The } u\text{-subproblem} \\ \quad u_{k+1} = \operatorname{argmin}_u \mathcal{J}(u, v_k, m_k, n_k) + \frac{\lambda_0}{2} \|b_k^0 + u - v_k\|_2^2 + \frac{\lambda_1}{2} \|b_k^1 + \Delta v_k - m_k\|_2^2 \\ \quad \quad + \frac{\lambda_2}{2} \|b_k^2 + \nabla v_k - n_k\|_2^2, \\ \text{The } v\text{-subproblem} \\ \quad v_{k+1} = \operatorname{argmin}_v \mathcal{J}(u_{k+1}, v, m_k, n_k) + \frac{\lambda_0}{2} \|b_k^0 + u_{k+1} - v\|_2^2 + \frac{\lambda_1}{2} \|b_k^1 + \Delta v - m_k\|_2^2 \\ \quad \quad + \frac{\lambda_2}{2} \|b_k^2 + \nabla v - n_k\|_2^2, \\ \text{The } m\text{-subproblem} \\ \quad m_{k+1} = \operatorname{argmin}_m \mathcal{J}(u_{k+1}, v_{k+1}, m, n_k) + \frac{\lambda_0}{2} \|b_k^0 + u_{k+1} - v_{k+1}\|_2^2 \\ \quad \quad + \frac{\lambda_1}{2} \|b_k^1 + \Delta v_{k+1} - m\|_2^2 + \frac{\lambda_2}{2} \|b_k^2 + \nabla v_{k+1} - n_k\|_2^2, \\ \text{The } n\text{-subproblem} \\ \quad n_{k+1} = \operatorname{argmin}_n \mathcal{J}(u_{k+1}, v_{k+1}, m_{k+1}, n) + \frac{\lambda_0}{2} \|b_k^0 + u_{k+1} - v_{k+1}\|_2^2 \\ \quad \quad + \frac{\lambda_1}{2} \|b_k^1 + \Delta v_{k+1} - m_{k+1}\|_2^2 + \frac{\lambda_2}{2} \|b_k^2 + \nabla v_{k+1} - n\|_2^2, \\ \text{The } b^i\text{-update } (i = 0, 1, 2) \\ \quad b_{k+1}^0 = b_k^0 + u_{k+1} - v_{k+1}, \\ \quad b_{k+1}^1 = b_k^1 + \Delta v_{k+1} - m_{k+1}, \\ \quad b_{k+1}^2 = b_k^2 + \nabla v_{k+1} - n_{k+1}. \end{array} \right.$$

The u -subproblem

This problem is

$$u_{k+1} = \operatorname{argmin}_{u \in R^l} \lambda \sum_{i,j} \frac{(u(i,j) - f(i,j))^2}{u(i,j)} + \frac{\lambda_0}{2} \|b_k^0 + u - v_k\|_2^2 \quad (17)$$

whose solution fulfills:

$$Au(i,j)^3 + Bu(i,j)^2 + C = 0,$$

where $A = 2\lambda_0$, $B = \lambda + 2\lambda_0(b_k^0(i, j) - v_k(i, j))$ and $C = -\lambda f(i, j)^2$. The polynomial

$$P(X) = AX^3 + BX^2 + C$$

is of degree 3 and hence has at least one real root. However, in our case, we can prove that it has exactly one real root which corresponds to the solution of (17). In fact, every root of $P(\cdot)$ is a solution of (17) which clearly is unique, because the strict convexity of the energy functional.

The v -subproblem

This problem is

$$v_{k+1} = \operatorname{argmin}_{u \in \mathbb{R}^l} \frac{\lambda_0}{2} \|b_k^0 + u_{k+1} - v\|_2^2 + \frac{\lambda_1}{2} \|b_k^1 + \Delta v - m\|_2^2 + \frac{\lambda_2}{2} \|b_k^2 + \nabla v - n\|_2^2$$

which is quadratic and it is solved through its optimality condition. It is trivial to calculate the solution of the last minimization problem, and which solves the following fourth-order equation:

$$\begin{aligned} & \lambda_1 D_{xx}(D_{xx}v) + 2\lambda_1 D_{xx}(D_{yy}v) + \lambda_1 D_{yy}(D_{yy}v) - \lambda_2 \left(\overleftarrow{D}_x(D_xv) + \overleftarrow{D}_y(D_yv) \right) \\ & + \lambda_0 v = \lambda_0(b_k^0 + u_{k+1}) + \lambda_1 D_{xx}(m_k - b_k^1) + \lambda_1 D_{yy}(m_k - b_k^1) + \lambda_2 \overleftarrow{D}_x(b_k^2 - n_k) + \lambda_2 \overleftarrow{D}_y(b_k^2 - n_k). \end{aligned} \quad (18)$$

To solve the previous fourth-order equation we can use the 2-dimensional discrete Fourier transforms. In fact, we have:

$$LS \cdot \mathcal{F}(v) = \mathcal{F}(RS),$$

where

$$LS = \lambda_1 \mathcal{F}(D_{xx}(D_{xx})) + 2\lambda_1 \mathcal{F}(D_{xx}(D_{yy})) + \lambda_1 \mathcal{F}(D_{yy}(D_{yy})) - \lambda_2 \mathcal{F}(\overleftarrow{D}_x(D_xv)) - \lambda_2 \mathcal{F}(\overleftarrow{D}_y(D_yv)) + \lambda_0 I.$$

The quantity RS is the right side of the (18) and “ \cdot ” means pointwise multiplication of matrices. Therefore, the discrete solution v can be obtained by applying the inverse of the discrete two-dimensional Fourier transform to the previous equation and we get:

$$v = \mathcal{F}^{-1}(RS/LS).$$

The m -subproblem

This problem is

$$m_{k+1} = \operatorname{argmin}_{m \in \mathbb{R}^l} \|m\|_p + \frac{\lambda_1}{2} \|b_k^1 + \Delta v_{k+1} - m\|_2^2$$

whose minimizer m_{k+1} is given explicitly by the following shrinkage-like formula:

$$m_{k+1} = \max \left\{ |b_k^1 + \Delta v_{k+1}| - \frac{|b_k^1 + \Delta v_{k+1}|^{p(\cdot)-1}}{\lambda_1 p(\cdot)}, 0 \right\} \frac{b_k^1 + \Delta v_{k+1}}{|b_k^1 + \Delta v_{k+1}|}.$$

The n -problem

This problem is

$$n_{k+1} = \operatorname{argmin}_{n \in \mathbb{R}^l \times \mathbb{R}^l} \|n\|_q + \frac{\lambda_2}{2} \|b_k^2 + \nabla v_{k+1} - n\|_2^2$$

whose minimizer n_{k+1} is given explicitly by the following shrinkage-like formula:

$$n_{k+1} = \max \left\{ \|b_k^2 + \nabla v_{k+1}\|_2 - \frac{\|b_k^2 + \nabla v_{k+1}\|_2^{q(\cdot)-1}}{\lambda_2 q(\cdot)}, 0 \right\} \frac{b_k^2 + \nabla v_{k+1}}{\|b_k^2 + \nabla v_{k+1}\|_2},$$

where $\|\cdot\|_2$ is the euclidean norm.

6 Numerical experiments

In the following subsection, we use some numerical experiments to examine the efficiency and robustness of the Algorithm 1. All experiments were run for a **double** noisy gray images to recover a true ones. All the images used here were downloaded from the internet and have a significant related to the purpose of this work to detect edges and thin-structure from medical images. The performance of the proposed approach is illustrated for multiplicative speckle noise removal and important features detection. We compare between the $p(\cdot)$ -Kirchhoff and the so-called TVL models i.e., $p(\cdot) \equiv q(\cdot) \equiv 1$:

$$\begin{cases} \alpha \Delta \left(\frac{\Delta u}{|\Delta u|} \right) - \beta \operatorname{div} \left(\frac{\nabla u}{|\nabla u|} \right) + 2\lambda D_u W(u, f) = 0, & \text{in } \Omega, \\ \frac{\partial \Delta u}{\partial n} = \frac{\partial u}{\partial n} = 0, & \text{on } \partial \Omega, \end{cases} \quad (19)$$

and with the “*Bi-Harmonic model*” i.e., $p(\cdot) \equiv q(\cdot) \equiv 2$.

Denosing performance is evaluated using the residual error which is on the order of 10^{-3} between two successive iterations for all the models and the number of iterations depends on the model, level of noise and images.

In Figure 1, we consider a medical image available from the internet which is corrupted by speckle noise with variance $\sigma^2 = 0.04$. The images illustrated below show the original image, noisy one, the topological gradient indicator for the second- and fourth-order PDE, and the variables exponent functions $p(\cdot)$ and $q(\cdot)$. Here, we test the efficiency and the performance of the proposed approach for important feature detection of blood vessels and veins. The images 1(c) and 1(d) show the topological gradient indicator for the second- and fourth-order operator, respectively. We can see that the topological gradient of the fourth-order PDE able to see more information about the objects presented here. However, the topological gradient indicator for the second-order PDE is carried for the detection of edges doesn’t perform to detect objects of smaller pixels. The images 1(e) and 1(f) show the variables exponent $q(\cdot)$ and $p(\cdot)$, respectively. The visualization of the variable exponents are depend on the topological gradient, however, for the important feature having the value of $q(\cdot)$ and $p(\cdot)$ near to 1 to slow down diffusion, we can also see from images 1(e) and 1(f) the values of the variable exponents ranging from 1 to 2 and the object detected by the second-order derivative are very thin.

We note that from Figure 1 the restoration result obtained by the $p(\cdot)$ -Kirchhoff model (see image 1(g)) gives better result than the TVL model (see image 1(h)) and the Bi-Harmonic model (see image 1(i)). We can deduce that the three models give good results with minor differences which are compared quantitatively by using the PSNR, SNR and SSIM indicators. We can also learn from the $p(\cdot)$ -Kirchhoff model that the variable exponents $p(\cdot)$ and $q(\cdot)$ can be considered as a sort of segmentation and important features detection.

Figure 2 shows the convergence of the split Bregman scheme for the three models. We compared between those models by using the number of iterations as function of the SSIM indicator. We can see that the SSIM indicator for the $p(\cdot)$ -Kirchhoff model speedely tends to 0.84 after 48 iterations. However, the SSIM indicator of the TVL model converges monotonically and slowly to 0.84 after 101 iterations. This isn’t surprising result since the $\Delta \left(\frac{\Delta \cdot}{|\Delta \cdot|} \right)$ and $\operatorname{div} \left(\frac{\nabla \cdot}{|\nabla \cdot|} \right)$ have slow impact on smoothness. The SSIM of the “Bi-Harmonic model” tends to 0.83 after only 39 iterations, it is due to the high frequency of the biLaplace, $\Delta^2 \cdot$, operator. From these images we can conclude that the “Bi-Harmonic model” is not stable with respect to the number of iterations, however at the iteration 42 it diverges (see Figure 2). The $p(\cdot)$ -Kirchhoff and TVL models give the same value of SSIM, their main deference is the number of iterations.

In Figure 3 we consider an image which contains only points to show the robustness of the topological gradient to detect the thin-structures like filaments and points. In image 3(c) the important feature of image are considered as edges having a jump across the discontinuity, however for image

3(e) the objects detected and do not have jump across the discontinuity.

We can show the performance of our model for a more specific ultrasound medical images. From Figure 4, we can see that the $p(\cdot)$ -Kirchhoff model gives a good result compared with the TVL model, however the result in 4(g) is very similar to the original one. From the figure 4(h), we can see that the TVL admits a strong smoothing rate on the medical images and one can also see white contrasts on some regions. When we zoom we can see in Figure 5 a comparison between the $p(\cdot)$ -Kirchhoff model, and the TVL model. For the TVL model we can see that the image is very smooth and we show artifacts (some white points) near the edges of the image and this due to the singularity of the total variation.

7 Conclusion

In this paper, we have presented a new approach to restore images corrupted by speckle multiplicative noise. The proposed approach combines the advantages of the topological gradient method for important feature detection and the anisotropic diffusion model based on the $p(\cdot)$ -Kirchhoff operator for the denoising. In the numerical computation, we used the split Bregman method in order to solve the nonlinear equation. The experiment results show the good quality in the recovering of the edges and thin structures as well as the image denoising.

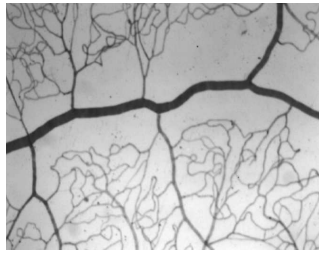
References

- [1] Mostafa Allaoui. Existence of three solutions for variable exponent elliptic systems. *ANNALI DELL'UNIVERSITA' DI FERRARA*, 61(2):241–253, 2015.
- [2] Samuel Amstutz and Jérôme Fehrenbach. Edge detection using topological gradients: A scale-space approach. *J. Math. Imaging Vis.*, 52(2):249–266, 2015.
- [3] Samuel Amstutz, Imen Horchani, and Mohamed Masmoudi. Crack detection by the topological gradient method. *Control and Cybernetics*, 34(1):81–101, 2005.
- [4] Samuel Amstutz, Antonio Andre Novotny, and Nicolas Van Goethem. Topological sensitivity analysis for high order elliptic operators. preprint, 2012.
- [5] Samuel Amstutz, Antonio Andre Novotny, and Nicolas Van Goethem. Topological sensitivity analysis for elliptic differential operators of order $2m$. *Journal of Differential Equations*, 256(4):1735–1770, 2014.
- [6] Gilles Aubert and Audric Drogoul. Topological gradient for a fourth order operator used in image analysis. *ESAIM: Control, Optimisation and Calculus of Variations*, 21(4):1120–1149, 2015.
- [7] Didier Auroux. From restoration by topological gradient to medical image segmentation via an asymptotic expansion. *Math. Comput. Model.*, 49(11):2191–2205, 2009.
- [8] Marino Belloni and Bernd Kawohl. A direct uniqueness proof for equations involving the p -Laplace operator. *Manuscripta Mathematica*, 109(2):229–231, 2002.
- [9] Martin Benning, Christoph Brune, Martin Burger, and Jahn Müller. Higher-order TV methods enhancement via Bregman iteration. *Journal of Scientific Computing*, 54(2-3):269–310, 2013.
- [10] Kristian Bredies, Karl Kunisch, and Thomas Pock. Total generalized variation. *SIAM Journal on Imaging Sciences*, 3(3):492–526, 2010.

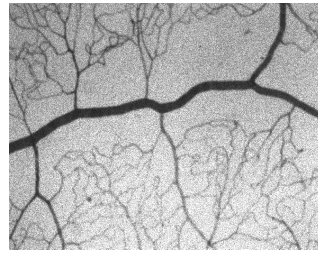
- [11] Jean Cea. Conception optimale ou identification de formes, calcul rapide de la dérivée directionnelle de la fonction coût. *ESAIM: Mathematical Modelling and Numerical Analysis*, 20(3):371–402, 1986.
- [12] Jean Cea, Stéphane Garreau, Philippe Guillaume, and Mohamed Masmoudi. The shape and topological optimizations connection. *Comput. Methods Appl. Mech. Engrg.*, 188(4):713–726, 2000.
- [13] Tony Chan, Antonio Marquina, and Pep Mulet. High-order total variation-based image restoration. *SIAM Journal on Scientific Computing*, 22(2):503–516, 2000.
- [14] Yunmei Chen, Stacey Levine, and Murali Rao. Variable exponent, linear growth functionals in image restoration. *SIAM Journal on Applied Mathematics*, 66(4):1383–1406, 2006.
- [15] Lars Diening, Petteri Harjulehto, Peter Hästö, and Michael Ruzicka. *Lebesgue and Sobolev spaces with variable exponents*. Springer, 2011.
- [16] Audric Drogoul. Numerical analysis of the topological gradient method for fourth order models and applications to the detection of fine structures in imaging. *SIAM Journal on Imaging Sciences*, 7(4):2700–2731, 2016.
- [17] David Edmunds and Jiří Rákosník. Sobolev embeddings with variable exponent. *Studia Mathematica*, 143(3):267–293, 2000.
- [18] David E Edmunds and Jiří Rákosník. Sobolev embeddings with variable exponent, ii. *Mathematische Nachrichten*, 246(1):53–67, 2002.
- [19] Abdelrachid El Amrouss, Fouzia Moradi, and Mimoun Moussaoui. Existence of solutions for fourth-order PDEs with variable exponents. *Electronic Journal of Differential Equations*, 2009(153):1–13, 2009.
- [20] Xianling Fan, Jishen Shen, and Dun Zhao. Sobolev embedding theorems for spaces $W^{k,p(x)}$. *Journal of Mathematical Analysis and Applications*, 262(2):749–760, 2001.
- [21] Xianling Fan and Dun Zhao. On the spaces $L^{p(x)}$ and $W^{m,p(x)}$. *Journal of Mathematical Analysis and Applications*, 263(2):424–446, 2001.
- [22] Roberta Filippucci, Patrizia Pucci, and Frédéric Robert. On a p-Laplace equation with multiple critical nonlinearities. *Journal de Mathématiques Pures et Appliquées*, 91(2):156–177, 2009.
- [23] Stéphane Garreau, Philippe Guillaume, and Mohamed Masmoudi. The topological asymptotic for PDE systems: The elasticity case. *SIAM J. Control Optim.*, 39(6):1756–1778, 2000.
- [24] Pascal Getreuer. Rudin-Osher-Fatemi Total Variation denoising using Split Bregman. *Image Processing On Line*, 2:74–95, 2012.
- [25] Pascal Getreuer. Total Variation deconvolution using split Bregman. *Image Processing On Line*, 2:158–174, 2012.
- [26] Pascal Getreuer. Total Variation inpainting using split Bregman. *Image Processing On Line*, 2:147–157, 2012.
- [27] Tom Goldstein and Stanley Osher. The split bregman method for l1-regularized problems. *SIAM journal on imaging sciences*, 2(2):323–343, 2009.

- [28] P. Harjulehto, P. Hästö, V. Latvala, and O. Toivanen. Critical variable exponent functionals in image restoration. *Applied Mathematics Letters*, 26(1):56 – 60, 2013.
- [29] Lamia Jaafar Belaid, Mohamed Jaoua, Mohamed Masmoudi, and Lassaad Siala. Application of the topological gradient to image restoration and edge detection. *Engineering Analysis with Boundary Elements Journal*, 32(11):891–899, 2008.
- [30] Zhengmeng Jin and Xiaoping Yang. A variational model to remove the multiplicative noise in ultrasound images. *J. Math. Imaging Vis.*, 39(1):62–74, 2011.
- [31] Karl Krissian, Ron Kikinis, Carl Fredrik Westin, and Kirby Vosburgh. Speckle-constrained filtering of ultrasound images. In *2005 IEEE Computer Society Conference on Computer Vision and Pattern Recognition (CVPR'05)*, volume 2, pages 547–552, 2005.
- [32] Fang Li, Zhibin Li, and Ling Pi. Variable exponent functionals in image restoration. *Applied Mathematics and Computation*, 216(3):870 – 882, 2010.
- [33] Peter Lindqvist. *Notes on the p -Laplace Equation*. University of Jyväskylä - Lectures notes, 2006.
- [34] Thanasis Loupas. *Digital image processing for noise reduction in medical ultrasonics*. PhD thesis, University of Edinburgh, UK, 1988.
- [35] Mohamed Masmoudi. The topological asymptotic. In R. Glowinski, H. Kawarada, and J. Periaux, editors, *Computational Methods for Control Applications*, volume 16 of *Math. Sci. Appl.*, pages 53–72. GAKUTO International, 2002.
- [36] Konstantinos Papafitsoros, Carola Bibiane Schoenlieb, and Bati Sengul. Combined First and Second Order Total Variation inpainting using Split Bregman. *Image Processing On Line*, 3:112–136, 2013.
- [37] Konstantinos Papafitsoros and Carola-Bibiane Schönlieb. A combined first and second order variational approach for image reconstruction. *Journal of Mathematical Imaging and Vision*, 48(2):308–338, 2014.
- [38] Michael Ruzicka. *Electrorheological fluids: modeling and mathematical theory*. Springer Science & Business Media, 2000.
- [39] Jan Sokolowski and Antoni Zochowski. On the topological derivative in shape optimization. *SIAM J. Control Optim.*, 37(4):1251–1272, 1999.
- [40] Carsten Steger. Extracting curvilinear structures: A differential geometric approach. In *European Conference on Computer Vision*, pages 630–641. Springer, 1996.
- [41] Carsten Steger. An unbiased detector of curvilinear structures. *IEEE Transactions on Pattern Analysis and Machine Intelligence*, 20(2):113–125, 1998.
- [42] Yilun Wang, Junfeng Yang, Wotao Yin, and Yin Zhang. A new alternating minimization algorithm for total variation image reconstruction. *SIAM Journal on Imaging Sciences*, 1(3):248–272, 2008.
- [43] Chunlin Wu and Xue Cheng Tai. Augmented lagrangian method, dual methods, and split bregman iteration for rof, vectorial tv, and high order models. *SIAM Journal on Imaging Sciences*, 3(3):300–339, 2010.

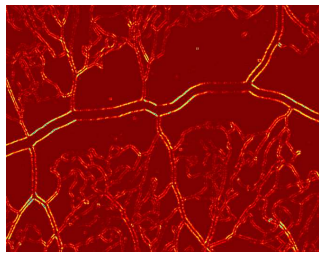
- [44] Y. L. You and M. Kaveh. Fourth-order partial differential equations for noise removal. *IEEE Transactions on Image Processing*, 9(10):1723–1730, 2000.
- [45] Vasilii Vasil'evich Zhikov. Averaging of functionals of the calculus of variations and elasticity theory. *Izvestiya: Mathematics*, 29(1):33–66, 1987.



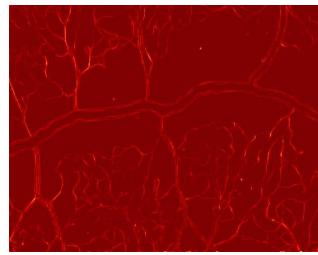
(a) Initial image



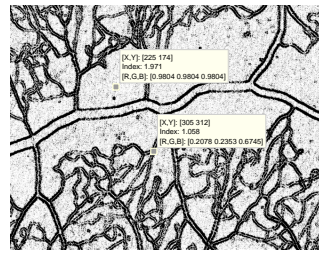
(b) SSIM= 0.17, PSNR= 17.39dB, SNR= 14.63dB.



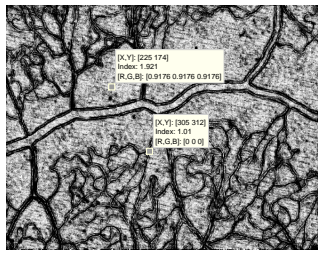
(c)



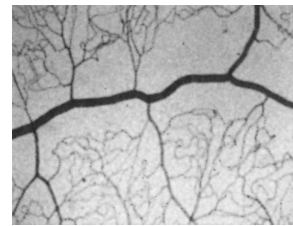
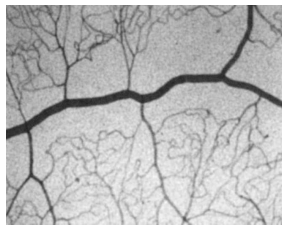
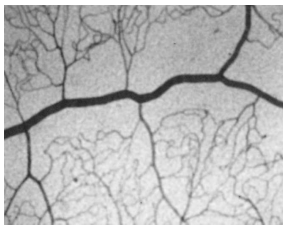
(d)



(e)



(f) The variable $p(\cdot)$



(g) SSIM= 0.847, PSNR= 29.3dB, (h) SSIM= 0.842, PSNR= 28.58dB, (i) SSIM= 0.837, PSNR= 27.79dB, SNR= 26.52dB, 48 iterations. SNR= 25.97dB, 101 iterations. SNR= 25.19dB, 39 iterations.

Figure 1: (a) Original image, (b) noisy one, (c) topological gradient for second-order, (d) topological gradient for fourth-order, (e) the variable $q(\cdot)$, (f) the variable $p(\cdot)$, (g) $p(\cdot)$ -Kirchhoff model, (h) TVL model and (i) “Bi-Harmonic” model.

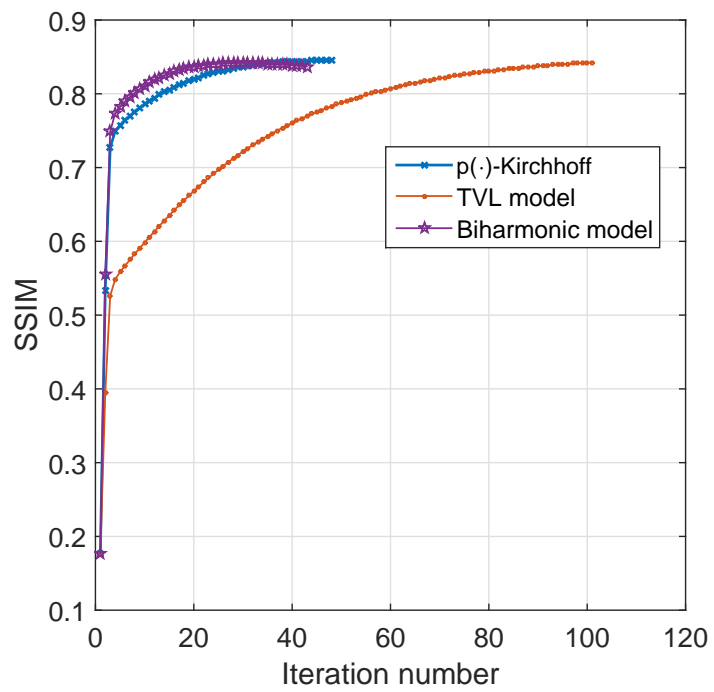
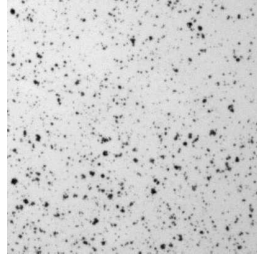
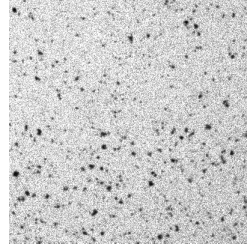


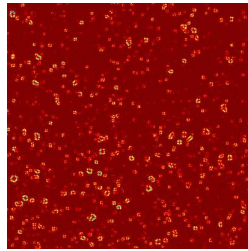
Figure 2: Convergence of split Bregman method (using image test in Figure 1).



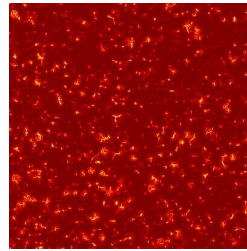
(a) Initial image



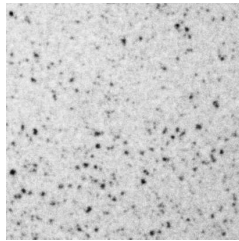
(b) SSIM= 0.18, PSNR= 16.77dB, SNR= 15.01dB.



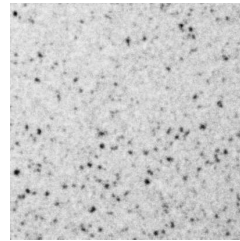
(c)



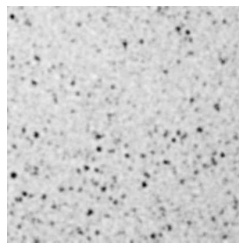
(d)



(e) SSIM= 0.7, PSNR= 25.74dB, SNR= 24.03dB, 41 iterations.



(f) SSIM= 0.66, PSNR= 23.44dB, SNR= 21.83dB, 57 iterations.



(g) SSIM= 0.67, PSNR= 24.41dB, SNR= 22.8dB, 32 iterations.

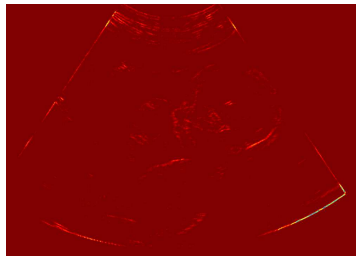
Figure 3: (a) Original image, (b) noisy one, (c) topological gradient for second-order, (d) topological gradient for fourth-order, (e) $p(\cdot)$ -Kirchhoff model, (f) TVL model and (g) “Bi-Harmonic” model.



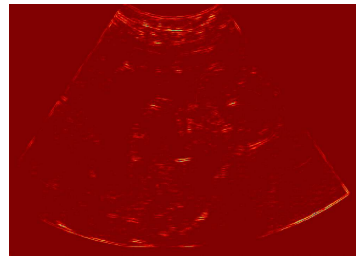
(a)



(b) SSIM= 0.72, PSNR= 26.21dB, SNR= 14.16dB.



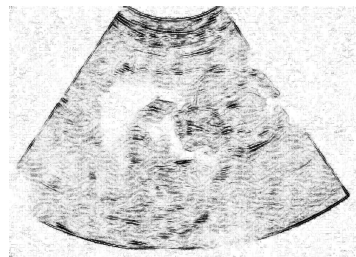
(c)



(d)



(e)



(f)



(g) SSIM= 0.96, PSNR= 38.29dB, SNR= 26.08dB.



(h) SSIM= 0.95, PSNR= 30.68dB, SNR= 20.33dB.

Figure 4: (a) Original image, (b) noisy one, (c) topological gradient for second-order, (d) topological gradient for fourth-order, (e) the variable $q(\cdot)$, (f) the variable $p(\cdot)$, (g) $p(\cdot)$ -Kirchhoff model, (h) TVL model.

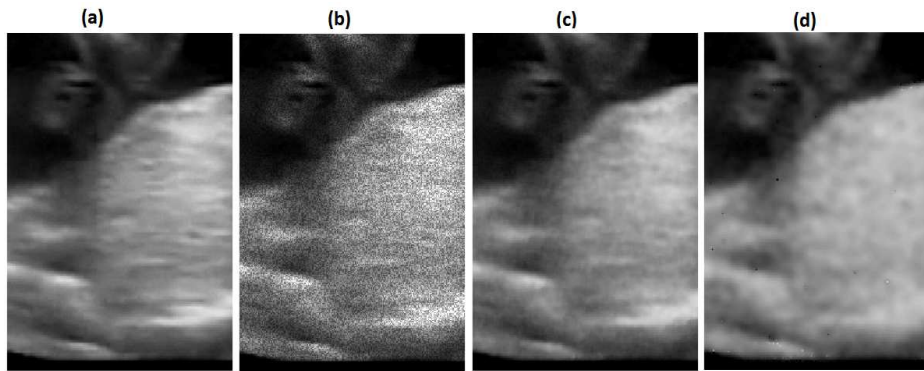


Figure 5: Zooming of Figure 4: (a) The original part, (b) the noisy one, (c) $p(\cdot)$ -Kirchhoff model, and (d) the TVL model.



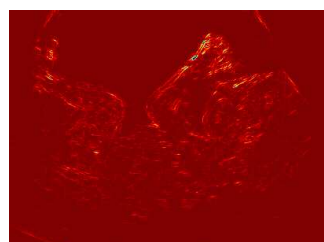
(a) Initial image



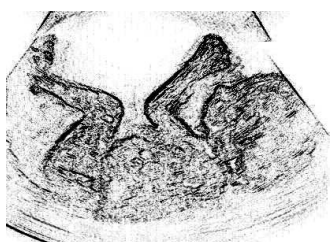
(b) SSIM= 0.55, PSNR= 21dB, SNR= 12.77dB.



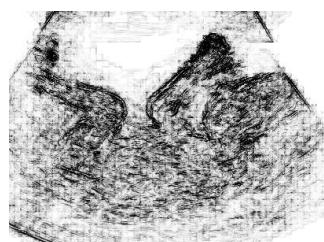
(c)



(d)



(e)



(f)



(g) SSIM= 0.868, PSNR= 30dB, (h) SSIM= 0.861, PSNR= 29.36dB, (i) SSIM= 0.867, PSNR= 29.91dB, SNR= 21.62dB, 44 iterations. SNR= 20.98dB, 51 iterations. SNR= 21.53dB, 46 iterations.

Figure 6: (a) Original image, (b) noisy one, (c) topological gradient for second-order, (d) topological gradient for fourth-order, (e) $p(\cdot)$ -Kirchhoff model, (f) TVL model and (g) “Bi-Harmonic” model.